



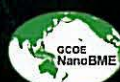
Japan-Portugal Nano-BME Symposium 2011

3 June 2011

Faculty of Engineering of the University of Porto (FEUP)

6 June 2011

Polytechnic Institute of Bragança
(Auditorium Alcino Miguel, ESTiG)



Tohoku University

FEUP FACULDADE DE ENGENHARIA
UNIVERSIDADE DO PORTO

ipb INSTITUTO POLITÉCNICO DE BRAGANÇA
Escola Superior de Tecnologia e Gestão

Analysis of the Cell-Free Layer in a Circular Microchannels: Trajectories of Labeled Red Blood Cells

Catarina Meireles¹⁾, Ana I. Pereira^{1,2)}, Tomoko Yaginuma¹⁾ and Rui Lima^{*1,3)}

1) Polytechnic Institute of Bragança, ESTiG/IPB, Bragança, Portugal.

2) ALGORITMI, Minho University, Guimarães, Portugal.

3) CEFT, Faculdade de Engenharia da Universidade do Porto (FEUP), Porto, Portugal..

E-mail: ruimec@ipb.pt



Abstract

In this experimental work, we measure the trajectories of the cell-free layer (CFL) by tracking labeled red blood cells (RBCs) flowing around the boundary of the RBCs core. The circular glass microchannels studied are 100 μm in diameter. The images are captured using a confocal system and are post-processed using Image J and MATLAB. The results suggest that the trajectories follow a polynomial function.

1. Introduction

The cell-free layer (CFL) is well known physiological phenomenon that happens at both in vivo in vitro blood flowing in microcirculation [1-4]. This phenomenon is due the red blood cells (RBCs) tendency to undergo axial migration due to the high shear stress around wall that forces the RBCs to move towards the center of the channel. Although there have been several studies on the measurement of CFL thickness, according to our knowledge there have been very few studies on the determination of CFL trajectory. The main purpose of the present work is to measure the measure several trajectories of the CFL by tracking labeled RBCs in 100 μm glass capillaries. This experimental study was performed using a confocal microscopy system together with image analysis techniques.

2. Materials and Methods

2.1. Working fluids and microchannel geometry

The working fluid used in this study was Dextran 40 (Dx-40; Otsuka Medicine) containing $12 \pm 2\%$ (12Hct) of human RBCs. The Hcts corresponded to the feed reservoir Hct and were measured using a hematocrit centrifuge (Kubota 3220) immediately before each experiment. The RBCs were labeled with a lipophilic carbocyanine derivative, chloromethylbenzamido (CM-Dil, C-7000, Molecular Probes). A detailed description about the procedure for labeling the human RBCs can be found elsewhere [3].

The microchannels tested in this study were 100- μm circular borosilicate glass microchannel fabricated by

Vitrocom (Mountain Lakes). The microchannel was mounted on a slide glass was immersed in glycerol to minimize the refraction from the walls.

2.2. Experimental set-up

The confocal micro-PTV system used in this study consists of an inverted microscope (IX71; Olympus) combined with a confocal scanning unit (CSU22; Yokogawa), a diode-pumped solid-state (DPSS) laser (Laser Quantum) with an excitation wavelength of 532 nm and a high-speed camera (Phantom v7.1; Vision Research). The microchannels were placed on the stage of the inverted microscope and by using a syringe pump (KD Scientific) a pressure-driven flow was kept constant ($Re \sim 0.008$). Additionally, by using a thermo plate controller (Tokai Hit) the temperature was set to $37^\circ\text{C} \pm 1$. More detailed information about this system can be found elsewhere [3, 5, 6].

2.3. Tracking RBC trajectory

The laser beam was illuminated from below the microscope stage through a dry 40 \times objective lens with a numerical aperture (NA) equal to 0.9. The confocal images were captured in middle of the capillary with a resolution of 640 \times 480 pixel at a rate of 100 frames/s with an exposure time of 9.4 ms. A manual tracking plugin (MTrackJ) [7] of an image analysis software (Image J, NIH) [8] was used to track the label RBCs. By using MTrackJ plugin, the bright centroid of the selected RBC was used through successive images. After obtaining series of x and y positions, data were exported for MATLAB and the *cftool* package was used to calculate the best function that approximates the numerical results. Fig. 1 shows the trajectories of a labeled RBC flowing around the edge of the RBCs core.

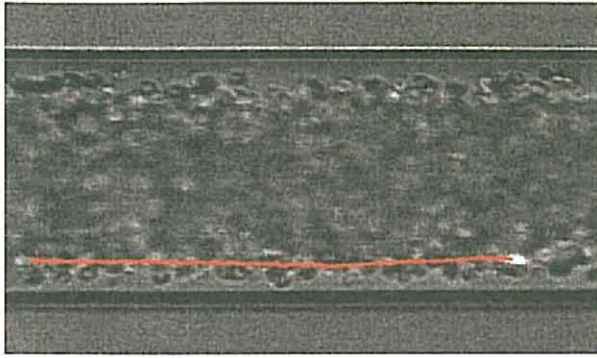


Fig. 1. Trajectory of a labeled RBC flowing around the boundary region between CFL and RBCs core.

3. Results and Discussion

This section presents numerical results concerning to the approximation of the data that was obtained using the technique described in the previous section.

We used the *cftool* package of MatLab software which is identified as the best function that approximates the data using the least squares technique. In the following table it is presented the error of least squares technique of the seven best approximations.

Table 1. Error of the seven best functions obtained with *cftool*.

Function	Error (um)			
Poly5	18,6327	6,8002	22,9216	18,0606
Fourier1	21,6219	11,0451	28,1591	20,6800
Poly4	22,9811	7,7465	26,8842	20,2669
Poly3	23,7068	8,2364	33,9576	24,1843
Exp2	23,7505	8,1408	34,0389	24,6697
Poly2	23,7738	12,2127	33,9702	25,7616
Power2	24,3397	24,6196	43,3759	51,3068

Considering the data of one cell, Fig. 3 shows the five best functions obtained with least squares method.

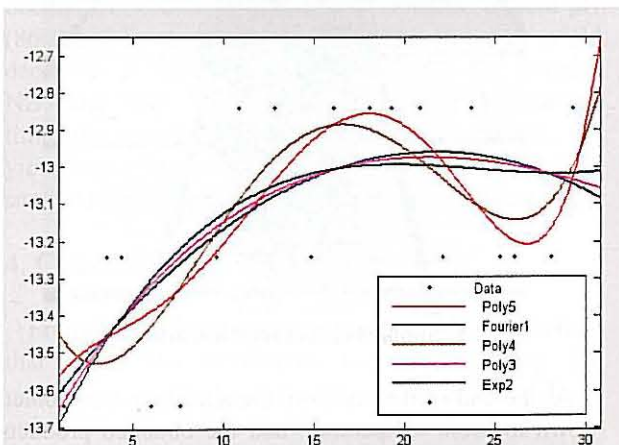


Fig. 3. Graph of the five best functions that define the trajectory of one cell.

Observing the Table 1 and Fig. 3 we can conclude that the best function that approximate the data is based on polynomial of degree five.

Acknowledgements

This study was supported in part by the following grants: International Doctoral Program in Engineering, from the Ministry of Education, Culture, Sports, Science and Technology of Japan (MEXT), 2007 Global COE Program "Global Nano-Biomedical Engineering Education and Research Network", Japan. Additionally, the authors also acknowledge the financial support provided by: PTDC/SAU-BEB/108728/2008, PTDC/SAU-BEB/105650/2008 and PTDC/EME-MFE/099109/2008 from the Science and Technology Foundation and COMPETE, Portugal.

References

- [1] Kim S, *et al.* A computer-based method for determination of the cell-free layer width in microcirculation. *Microcirculation* **13**, 199-207, 2006.
- [2] Lima R, *et al.* Radial dispersion of red blood cells in blood flowing through glass capillaries: role of hematocrit and geometry. *Journal of Biomechanics*, **41**, 2188-2196, 2008.
- [3] Lima R, Ishikawa T, Imai Y, Takeda M, Wada S, and Yamaguchi T. Measurement of individual red blood cell motions under high hematocrit conditions using a confocal micro-PTV system. *Annals of Biomedical Engineering* **37**, 1546-59, 2009.
- [4] Fujiwara H, Ishikawa T, Lima R, Matsuki N, Imai Y, Kaji H, Nishizawa M and Yamaguchi T. Red blood cell motions in high-hematocrit blood flowing through a stenosed microchannel. *Journal of Biomechanics* **42**, 838-843, 2009.
- [5] Lima, R. *et al.* Confocal micro-PIV measurements of three dimensional profiles of cell suspension flow in a square microchannel. *Measurement Science and Technology* **17**, 797-808, 2006.
- [6] Lima R. *et al.* In vitro blood flow in a rectangular PDMS microchannel: experimental observations using a confocal micro-PIV system. *Biomedical Microdevices* **10**, 153-67, 2008.
- [7] Meijering E, Smal I, and Danuser G. Tracking in molecular bioimaging. *IEEE Signal Process. Mag* **23**, 46-53, 2006.
- [8] Abramoff M, Magelhaes P, and Ram S. Image Processing with ImageJ. *Biophotonics International*, **7**, 11, 36-42, 2004.